

### AIN SHAMS UNIVERSITY

### FACULTY OF ENGINEERING

MECHATRONICS ENGINEERING

# Hand Prosthetic Controlled System Based on Signal Pattern Recognition of Electroencephalography

A Thesis submitted in partial fulfillment of the requirements of the

M.Sc. in Mechanical Engineering

By

Ahmed AlaaEldin Ibrahim Khalil

B.Sc., Mechanical Engineering, Mechatronics Engineering Department Helwan University, 2010

Supervised by

Prof. Dr. Farid Abdel Aziz Tolbah Prof. Dr. Ann Ali Abdel kader Dr. Mohammed Ibrahim M. H. Awad

Cairo - (2017)



#### AIN SHAMS UNIVERSITY

#### FACULTY OF ENGINEERING

# Hand Prosthetic Controlled System Based on Signal Pattern Recognition of Electroencephalography

By

### Ahmed AlaaEldin Ibrahim Khalil

B.Sc., Mechanical Engineering, Mechatronics Section Helwan University, 2010

#### **EXAMINERS COMMITTEE**

Name	Signature
Prof. Abbas A. Dehghani Sanij	
Chair in Bio-Mechatronics & Medical Robotics, University of Leeds	
Prof. Sherif Ali Mohamed Hammad	
Professor of Computers and Systems Engineering, Ain Shams University	
Prof. Farid Abdel Aziz Tolbah	
Professor of Design and Production Engineering, Ain Shams University	

Date: 8//10/2017

### Statement

This thesis is submitted as a partial fulfillment of M.Sc. degree in Mechanical engineering, Faculty of Engineering, Ain Shams University.

The author carried out the work included in this thesis and no part of it has been submitted for a degree or qualification at any other scientific entity.

#### Ahmed AlaaEldin Ibrahim Khalil

Signature

.....

### Researcher Data

Name: Ahmed AlaaEldin Ibrahim Khalil

Date of birth: 03/05/1987

Place of birth: Cairo, Egypt

Academic Degree: BSc. In mechanical Engineering

Field of specialization: Mechatronics Engineering

University issued the degree: Helwan University

Date of issued degree: 2010

**Current Job:** Demonstrator at Mechatronics Department, The Egyptian Academy for Engineering and Advanced Technology.

### Abstract

Electroencephalography (EEG) motor imagery (MI)-based Brain Computer Interface (BCI) systems have been recently employed to enhance the quality of life of disabled people. However, to naturally trigger particular applications (i.e. upper limb prostheses), independent BCIs appeal further paradigms to involve realistic motor imagery tasks. On the other hand, most of the EEG recording systems are clinical so that they cannot be integrated with such real time BCI mobility. In terms of machine learning, this work is intended to investigate into a realistic and intuitive motor imagery-based BCI for right hand using Consumergraded EEG acquisition devices. The present study proposes an approach to classify imagined hand gesture tasks, including the water glass gesture and the index pointer gesture of the right hand using OPENBCI as a consumer-grade EEG acquisition device. For three subjects, the data recorded by OPENBCI were sampled with a sampling rate of 250 Hz. The Minimum Redundancy Maximum Relevance (MRMR) technique was implemented as a feature selection method along with the Support Vector Machine (SVM) algorithm for classification. By obtaining a maximum classification accuracy of 91.7%, the results shown the feasibility of such Brain Computer Interface systems to detect different motor imagery tasks for the right hand. Consequently, upper limb prostheses could be manipulated using the intended motor imagery tasks.

**Key words**: Brain Computer Interface (BCI), Feature Selection, OPENBCI, MRMR, ERD.

## Acknowledgment

Foremost, I would like to express my sincere gratitude to my supervisors Prof. Dr. Farid Tolbah, Prof. Dr. Ann A. Kadir and Dr. Mohamed I. Awad for their continuous support of my master degree and for guiding and motivating me to produce this research work.

I would like to especially thank Dr. Mohamed Awad for suggesting the topic of the thesis to me and sharing with me all his profound knowledge of it. His guidance helped me in all the time of research and writing of this thesis. I could not have imagined having a better advisor and mentor for my M.Sc. study.

I would like to thank in advance Eng. Mohamed Mostafa for his financial aid to purchase the experimental equipment. I will never forget all the deeds you have done for me.

I would like to thank Eng. Ahmed Abdelshakour, Eng. Ahmed El-Rakaybe, Eng. Mostafa Arafa and Eng. Mohamed Zarzoura for helping me in the admission affairs and for the motivating discussions.

I would like to thank Dr. Hussein Fouad for encouraging and supporting me.

I would not have reached this point without the infinite support of my family. I would like to thank my mother, father and my two little sisters for being there for me and for their continuous encouragement to finish my work in the best way possible.

At last but not least, I give my dearest gratitude to my wife, who gave me all the patience and passion to fulfill this work and supported me spiritually throughout my life.

# Contents

Statement	iii
Researcher Data	iv
Abstract	v
Acknowledgment	vi
Contents	vii
List of Figures	X
List of Tables	xiii
List of Abbreviations	xiv
Chapter 1: Introduction	1
1.1. Motivation	1
1.2. Objectives	2
1.3. Scope of the work	2
1.4. Organization of the thesis	3
1.5. Contributions of this work	4
Chapter 2: Background	5
2.1. Brain activity measurements	5
2.1.1. Brain anatomy	7
2.1.2. Brain Function	11
2.1.3. Frequency ranges	12
2.2. Neuro-physiological phenomena used for driving BCIs	15
2.2.1. Evoked Potentials	16
2.2.2. Spontaneous potentials	17
2.3. BCIs as a machine learning approach	20
2.4. Signal pre-processing	21
2.4.1. Temporal filters	22
2.4.2. Spatial filters	24
2.5. Feature extraction	29
2.5.1. Signal amplitude	
2.5.2. Autoregressive model	
2.5.3. Band power method	
2.5.4. Power spectral density	
2.6. Feature selection and dimensionality reduction	

2.6.1. Principle Component Analysis	32
2.6.2. Minimum Redundancy Maximum Relevance	33
2.7. Classification	34
2.7.1. Linear Discriminant Analysis	35
2.7.2. Support Vector Machine	36
2.7.3. Other classifiers	38
2.8. Control approaches for upper limb prosthesis	38
2.8.1. Upper limb amputation	38
2.8.2. EMG-controlled upper limb prosthetics (Advances and lim	nitations)39
2.8.3. Recent progress in motor imagery based BCIs	40
2.8.4. MI-based BCIs for restoring upper limb disability	41
2.8.5. Gap of knowledge	42
Chapter 3: EEG Experimental Setup for Multi-Class MI-based BCIs	44
3.1. Problem Statement	44
3.2. EEG signal acquisition specifications	45
3.3. Electrodes placement	48
3.4. Experimental paradigm	51
3.5. Data recording	53
3.6. Evaluation	54
3.7. Summary	59
Chapter 4: Classification and feature ranking of the right hand mot	or imagery
tasks using MRMR	60
4.1. Problem statement	60
4.2. Methodology	62
4.2.1. Signal pre-processing	62
4.2.2. Spatial filtering using ICA	62
4.2.3. Feature extraction	64
4.2.4. Feature Selection Method: Minimum Redundancy	Maximum
Relevance (MRMR)	65
4.2.5. Classification using an SVM model	67
4.3. Validation	68
Chapter 5: Towards the Classification of Multi-Class EEG-Based Ha	and Gesture
Motor Imagery tasks using EEG source Imaging Estimation.	70
5.1. Problem Statement	70
5.2. Methodology	71

5.2.1. Arcitecture of Source Image-based BCI71
5.2.2. Estimation of source images71
5.2.3. Featuring and Classification modelling75
Chapter 6: Results and discussion78
6.1. Results: Classification and feature ranking of the right hand motor imagery
tasks using MRMR78
6.1.1. Influence of time window78
6.1.2. Influence of Dimensionality reduction methods
6.1.3. Classification accuracy for a 2-class BCI system79
6.1.4. Subject dependent vs subject independent BCIs83
6.2. Results: towards the Classification of Multi-Class EEG-Based Hand
Gesture Motor Imagery, tasks using EEG source Imaging Estimation84
6.2.1. Influence of time window
6.2.2. Influence of vertices number
Chapter 7: Conclusion and Future Work
7.1. Conclusion
7.2. Future Work
Bibliography

# List of Figures

Figure 2-1: Strategy and scheme of a brain–computer interface (BCI) system.			
Signals produced by brain activity are measured from the scaln. Features are			
extracted and quantified from the signals that best represent the user's intent			
(from [4])			
Figure 2-2: Examples of brain activity recording techniques (A) EEC signal sour			
is measured non-invasively with electrodes placed over the scalp. (B) ECoG			
electrodes are placed either outside the dura mater (enidural ECoC) or under			
the dura mater (subdural FCoC) and can record neural activity on the			
continued surfaces (C) Introductional microsologitudes ponetrate the contex and			
contracts surface. (C) intracortical inici detectrodes penetrate the cortex and			
can record action potentials from individual or small populations of neurons			
within the cortex (from [11])8			
Figure 2-3: The basic components of the neuron9			
Figure 2-4: A demonstration of the interconnection between to neuron cells in the			
cerebral cortex10			
Figure 2-5: The three basic layers of the brain comprising their estimated			
resistivity and thickness (From [13])11			
Figure 2-6: The main parts of the brain (From [13])12			
Figure 2-7: Rhythms of the brain as quantified by EEG in normal amplitudes			
(from [13])14			
Figure 2-8: The relative EEG power spectrum with respect to the EEG frequency			
bands (from [16])			
Figure 2-9: Emergence of SSVEP while stimulation exists with frequencies of 17 Hz			
(plain line) or 20 Hz (dotted line) (from [19])16			
Figure 2-10: P300 exists when the desired target is displayed (From [23])			
Figure 2-11: ERD and ERS in $\mu$ , and $\beta$ rhythms acquired by the C3 electrode			
during right finger lifting (from [29])			
Figure 2-12: Origin of ERD in the brain following left hand and right hand motor			
imagery (From [35]) 19			
Figure 2-13: An otlas for the origin of the different motor tasks (from [35]) 20			
Figure 2-13. An atlas for the origin of the unferent motor tasks (from [33])			
righte 2-14. Doo perception, unit separation of the EEG waveforms (Ifold [15]).			
Eigure 2 15: Independent Component Analysis of FEC (From [54])			
Figure 2-15: Independent Component Analysis of EEG (From [54]).			
Figure 2-10: Principle stages of source imaging (from [62])28			

Figure 2-17: An LDA-based hyperplane for binary classification problem (From
[89])
Figure 2-18: An SVM-based hyperplane for discriminating two classes (From [89]).
Figure 3-1: The 32-bit OPENBCI board (From [119])47
Figure 3-2: Connecting the electrodes to the OPENBCI board (From [119])47
Figure 3-3: The main components mounted to the board (From[119])48
Figure 3-4: 10/20 system of the total front-back distance (From [120])
Figure 3-5: 10/20 system of total right-left distance (From [120])50
Figure 3-6: The 10/20 international electrode-positioning standard51
Figure 3-7: Aspect of the experimental sessions
Figure 3-8: Experimental scenario of collecting motor imagery EEG dataset using
OPENVIBE platform
Figure 3-9: Trial timeline for Motor Imagery task data53
Figure 3-10: EOG oscillatory patterns during demo session for subject no.255
Figure 3-11: EMG signals during the demo session for subject no. 2
Figure 3-12: An example of bad and good EEG trials, where the event types 1098,
770 and 769 are the class labels57
Figure 3-13: Number of bad trials performed in each class
Figure 4-1: A block diagram of the proposed approach61
Figure 4-2: Topographic 2-D map of the eight Independent Components (IC's) for
all of the subjects64
Figure 4-3: Scalp map for the average of the selected Independent Components of
the three subjects in the time scale of 100 to 1800 <i>msec</i> 64
Figure 4-4: Flowchart of number of features and classifier parameters optimization
approach using K-fold cross validation69
Figure 5-1: Architecture of the proposed EEG source image-based BCI system for
classification of the three MI tasks72
Figure 5-2: The collin27 MRI template used as a head model for the three subjects.
74
Figure 5-3: (a) the averaged scalp oscillatory pattern for the trials related to the
water glass gesture and the correspondent equivalent dipole activities. (b) The
averaged scalp oscillatory pattern for the trials related to the index pointer
gesture and the correspondent equivalent dipole activities. (c) The averaged
scalp oscillatory pattern for the trials related to the rest state and the
correspondent equivalent dipole activities77
Figure 5-4: The corresponding cortical ROI that selected for all the subjects77

Figure 6-1: Mean classification performance of each window size for the three
subjects using MRMR79
Figure 6-2: Classification performance of the two motor imagery tasks using the
MRMR and PCA feature selection methods plotted as a function of the
number of best features used. The maximum accuracy for MRMR and PCA
method was achieved when using 58 and 70 of the top features respectively80
Figure 6-3: Confusion matrices for the MRMR and PCA methods at their
respective peak overall accuracy (Water glass gesture, Index pointer gesture).
Figure 6-4: Time Frequency representation of P3 location during index pointer
gesture and water glass gesture patterns81
Figure 6-5: A comparison between the classification performance of each subject
and the subject-independent trials83
Figure 6-6: Influence of time window on the classification accuracy for each
subject
Figure 6-7: Influence of the amount of vertices on the classification accuracy for
each subject

Table 2-1: THE LOBES OF THE BRAIN, THEIR ABBREVIATIONS AND	
THEIR FUNCTIONS.	.13
Table 2-2: A SUMMARY OF PREVIOUS EEG-BASED BCI STUDIES USING	
DIFFERENT FEATURE SELECTION ALGORITHMS	.43
Table 3-1: Overview of the data sets collected by BCI research center	.45
Table 3-2: List of the event types used to mark the steps of the experimental	
paradigm	.56
Table 3-3: Number of bad and good trials performed by the subjects for each	
session	.58
Table 6-1: THE WINDOW SIZE AND THE COMPUTATIONAL TIME FOR	
THE MAXIMUM ACCURACY FOR EACH SUBJECT WHILE APPLYIN	G
MRMR AS A FEATURE SELECTION METHOD	.78
Table 6-2: A SUMMARY OF PREVIOUS EEG-BASED BCI STUDIES USING	
DIFFERENT FEATURE SELECTION ALGORITHMS COMPARED TO	
THE PROPOSED APPROACH	.82

# List of Abbreviations

AR	Auto Regressive
BP	Band Power
DBN	Dynamic Bayesian Network
LDA	Linear Discriminant Analysis
MD	Mahalanobis Distance
MI	Motor Imagery
MRMR	Minimum Redundancy Maximum Relevance
PCA	Principle Component Analysis
PSD	Power Spectral Density
SVM	Support Vector Machines
TFR	Time-Frequency Representation

## Chapter 1: Introduction

### 1.1. Motivation

It was estimated that there are nearly 10 million amputees all over the world. Among the world population of amputees, there are 3 million population who have upper limb amputation [1]. Thanks to the recently astonishing advances of the interaction between human and computers, multidisciplinary paradigms have been revealed to improve the quality of upper limb amputee's life. Among those paradigms, Brain Computer Interfaces are novel technologies that are devoted to assist the people with severe disabilities. Nowadays, BCIs are widely utilized in different paradigms such as rehabilitation, mental spellers, motor restoration, clinical diagnoses and mental gaming.

Among the last two decades, investigations have been diversely conducted exploiting the non-invasiveness property of Electroencephalography (EEG) signals. These studies have shown promising outcomes for helping people with different cases of disability. However, BCIs experience outstanding issues as the complexity of the disability increases.

Upper limb amputations are considered one of the most severe disabilities, due to the intervention of the arm in most of the daily life activities. Moreover, upper limbs perform in such flexible and dexterous pathways. Therefore, relative BCIs appeal further paradigms to, approximately, retrieve the functions of the amputated upper limb. In other words, diverse investigations of BCIs should be developed to trigger prosthetics by adopting the following aspects:

- BCIs should be based on recognizing realistic, voluntary and intuitive motor imagery tasks.
- Real-time BCIs should be accomplished by means of real-time computational performance.
- BCIs are not generalized yet, as the EEG waveforms are known of the non-stationarity and the low spatial resolution.