

Dosimetry Study of Physical Parameters for Flattening Filter Free and Standard Photon Beam Energies in Radiotherapy By

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A thesis submitted in conformity with the requirement for M.Sc. in Science (Physics - Radiation Physics), Faculty of Women for Arts, Science and Education.

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Submitted for partial fulfillment of M.Sc. Degree in Science (Physics – Radiation physics), Faculty of Women for Arts, Science and Education.

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يسُمُ اللهِ الرَّحْهِنِ الرَّحِيمِ

تُل لَوْ لَانَ الْبَهْرُ بِرَاوَا لِلْلِمَاتِ رَبِّي لَنَفْرَ الْبَهْرُ تَبَلَ أَنْ تَنْفَرَ لَلْبَهْرُ بَيْل وَلَوْ هِ نُنَا بِيشُلِهِ مَرَوَا ﴿١٠٩﴾ ثَنَ اللهُ يَرْمَى لِآلِيَّ النَّمَا إِلَاهُ فَهُ عَلَى اللهُ يَرْمَى لِآلِيَّ النَّمَا إِلَاهُ فَهُ اللهُ يَرْمَى لِآلِيَّ النَّمَا إِلَاهُ فَهُ اللهُ يَرْمَى لِآلِيَّ النَّمَا إِلَاهُ فَهُ اللهُ يَرْمَى لِآلِهِ النَّمَا اللهُ فَهُ اللهُ يَرْمَى لِآلِيَّ النَّمَا اللهُ فَهُ اللهُ عَمَلًا اللهُ وَالْمِرُ أَنْ مَن لَانَ يَرْمُو لِقَاءِ رَبِّهِ الْمَرَا ﴿ ١١ ﴾ مَالِمًا وَآلِي شَرِك بِعِبَاوَةٍ رَبِّهِ أَمَرًا ﴿ ١١ ﴾ مَالِمًا وَآلَ يُشْرِك بِعِبَاوَةٍ رَبِّهِ أَمَرًا ﴿ ١١ ﴾

[سورة الكهف]

Acknowledgements

I am kneeling obsequiousness to ALLAH thanking HIM for showing me the right way. Without God help, my efforts would have gone astray. It was through the grace of God that I was able to acquire this great accomplishment. Thanks also for a person I love him very much, the Prophet Mohammed {God's praise and peace upon}.

Great thanks to the Head of Physics Department for her kind help and continuous encouragement for me and all young scientists in our department.

Also, I wish to express all my deepest and sincerest gratitude to

Prof. Dr. Amal Mahmoud El-Shershaby (Prof. of Radiation Physics, Physics Depart., Faculty of Women for Arts, Science, and Education, Ain -Shams University). I am deeply indebted to her for her enormous patience, guidance, and support throughout the work program. My inspiration came from her passion for research and her confidence in my abilities. Working under her leadership in such an exciting field was both educationally and professionally enriching. As a model researcher, I look up to her for inspiration in my professional career.

I wish to express my deepest sincerest thanks to Prof. Dr. Hoda Abdel-Moniem Ashry (Prof. of Radiation Physics, National Center for Radiation Research and Technology, AEA.). for her capable supervision, guidance that helped enhancing my understanding of this field and who has given me much guidance necessary for this project,

and done so with a great deal of patience and valuable insight. She has been the driving force of this project.

I would also like to extend a special thanks to Dr. Khaled Mohamed El Shahat (Ass. Prof. of Medical Radiation Biophysics, Physics Depart., Faculty of Medicine, Al - Azhar University), who was more helpful, understanding, and enjoyable to work with throughout the course of the work, and for his capable supervision, fruitful guidance, encouragement, ideas, endless help and many illuminating discussions through the course of the investigation.

I would also like to thank the Radiation Laboratory team, Physics Department, Women Faculty, Ain Shams University for supporting this work.

Finally, I would like to thank my family, for their support, encouragement, and understanding throughout my M.Sc.'s research.



To

My parents (Father and
Mother),
My brothers,
My wife,
My cognates,
My professors
and

My colleagues

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ABSTRACT

Abstract

Recently started to be used in radiotherapy clinical practice the Flattening filter free (FFF) beams generated by medical linear accelerators. Flattening filter free beam have a fundamental physical parameter differences with respect to the standard filter flattened (FF) beams, making the generally used dosimetric parameters and definitions not always viable.

The current study will propose study for some dosimetric parameters for use in quality assurance of FFF beams generated by medical linacs in radiotherapy.

The main characteristics of the photon beams have been analyzed using specific data generated by a Varian TrueBeam linac having both FFF and FF beams of 6 and 10 MV energy, respectively and MP3 water tank, a large size, remote-controlled To operate the tank, MEPHYSTO version (mc2) control software from PTW for an automatic positioning of the MP3 water tank via stepper motor control and TBA electronics are required and Semiflex Ionization Chambers 31010. The beam was adjusted and the gantry angle was kept at zero degrees and to ensure that the beam was parallel to the central axis; measurements were performed at various depths and various field size.

To investigate the changes in the beam spectrum sample depth dose (DD) curves were measured to compare with standard data we found that there's significant differences between FFF and standard photon beam.

The softer spectra of the flattening filter free beam due to Production of contaminant electrons also affects depth doses beyond d_{max} leads to a steeper drop in dose deposition beyond the depth of maximum dose (d_{max}), also differences due to this are mainly observed in the surface region, show

that there is a slight increase in surface dose with the flattening filter removed and we found that the depth-dose depends on the flattening filter, and field size dependence of surface dose is smaller for FFF than FF and the depth of maximum dose shows weak dependence on field size variation for the FFF beam ,depths of dose maxima for flattened and unflattened beams did not deviate by more than 2mm .

Definitions for dose profile parameters are suggested starting from the renormalization of the FFF with respect to the corresponding FF beam. From this point the flatness concept has been translated into one of "unflatness" and other definitions have been proposed, maintaining a strict parallelism between FFF and FF parameter concepts.

Beam profiles of FFF beam differ significantly from the FF beam. The central peak in the beam profiles of FFF beam is pronounced only for medium to large field sizes. The higher energy is the more pronounced in the central peak. We found that outside the treatment field the doses are lower for non-flattened beams due to the reduction in out-of-field scatter. This would effectively act to reduce the dose to surrounding normal tissues.

The shape of the beam profile of a FFF beam changes slightly with depth due to a significantly reduced off-axis softening effect and hence the depth dose characteristic remains almost constant across the field even for large field sizes.

The quality controls used in establishing a quality assurance program when introducing FFF beams into the clinical environment are given here, keeping them similar to those used for standard FF beams and, recommendation for introduction of FFF beams into a clinical radiotherapy application for breast cancer patient as best example for comparison between FFF and FF for good dose distribution and coverage for target volume.

In summary, although there are a number of advantages of using a FFF beam especially for advanced radiotherapy techniques there are a few challenges (e.g., criteria for beam quality evaluation and penumbra, establishment of dosimetry methods, and consequences of photon target burn-up) which need to be addressed for establishing this beam as an alternate to the FF beam.

List of Symbols & Abbreviations

BSF Backscatter Factor

CAX Central Axis

CIAO Complete Irradiation Area Outline

D_{max} Depth of Maximum Dose

DVH Dose-Volume Histogram

DMI Digital Megavolt Imagers

EBRT External Beam Radiotherapy

EPID Electronic Portal Imaging Device

IBRT Internal Beam Radiotherapy

FFF Flattening Filter Free

FS Field Size

GR Gantry Rotation

GA Gantry Angle

IMRT Intensity Modulated Radiotherapy

ITP Inverse Treatment Planning

LINAC Linear Accelerator

MLC Multi leaf Collimator

MU Monitor Unit

OAD Off-Axis Distance

OAR Off-Axis Ratio

OAR Organ at Risk

OF Output Factor

PDD Percentage Depth Dose

List of Symbols & Abbreviations

PDIP Portal Dose Image Prediction

PTV Planning Tumor Volume

SAD Source-Axis Distance

SCD Source-Collimator Distance

SDD Source -Diaphragm Distance

SF Scatter Factor

SSD Source-Surface Distance

TD Target Dose

TPS Treatment Planning System

TV Target Volume

VMAT Volumetric Modulated Arc Therapy